Development of a submillimeter portable gammaray imaging detector, based on a GAGG:Ce silicon photomultiplier array

E. Kefalidis¹, I. Kandarakis^{1, 2}, E. David^{1, 2}*

 ¹Department of Biomedical Engineering, University of West Attica, Athens, Greece
²Radiation Physics, Materials Technology and Biomedical Imaging Laboratory, Department of Biomedical Engineering, University of West Attica, Athens, Greece,



9 - 12 October 2018



- ✓ The aim of this study is to investigate the behavior of the ArraySL-4 (4x4 array) SiPM coupled to a 1mm² GAGG:Ce pixellated scintillator array for possible applications in small-animal PET scanner dedicated to mouse brain.
- ✓ Evaluation was carried out with ²²Na & ¹³⁷Cs radioactive sources and results regarding intrinsic spatial resolution, energy resolution and peak to valley ratio are presented.

Introduction

- ✓ <u>GAGG:Ce scintillator crystal</u> has high density of 6.63 g/cm³, high light output (~46000 ph/MeV) and fast scintillation decay time (~80 ns).
- ✓ SiPM arrays are very flexible and can be used in the design of a dedicated mice PET head detectors.





Materials and Methods I

	SiPM characteristics			
	Company name	SensL		
	Model	ArraySL-4		
it we	Number of pixels	16		
	Active area	13.4 mm ²		
	Pixel size	3 x 3 mm ²		
	Cell size	35 μm		
	Cells per pixel	4774		
	Bias Voltage	+29.5V		
	Gain	10 ⁶		
	Photon Detection Efficiency at 520nm	15 %		

✓GAGG:Ce 12x12 scintillator array, with 1x1x10mm³ crystal size elements.

✓ The array has pitch 1.1mm with 0.1mm thickness of BaSO₄ reflector material. The coupling material used was optical grease (BC-630).

Materials and Methods II

✓A symmetric resistive charge division circuit reduces the 16 pixel outputs to 4 position signals

- 1. a two-stage charge division resistor circuit reduces the 16 output channels of SiPM at 8 by equally splitting them in a resistive matrix (4 rows-X, 4 columns-Y),
- 2. into 4 position signals (Xa, Xb, Ya, Yb) by a division network of weighting resistors.



Materials and Methods III

✓The 4 position signals were amplified and digitized using free running ADCs (50MHz sampling rate).

✓An FPGA (Spartan 6 LX150T) was used for triggering and signal processing of the pulses.

✓Trigger signal was produced when the sum of the four in coming samples exceeded a given digital threshold (150mV).

✓All the experiments conducted inside a black box under room temperature conditions.

Results under ²²Na excitation



Top: Raw image of the 12x12 GAGG:Ce scintillator array and a horizontal line profile of the scintillator elements under ²²Na excitation;

Bottom: Energy spectra of the two 2 pixels.

Results under ¹³⁷Cs excitation



Top: Raw image of the 12x12 GAGG:Ce scintillator array and a horizontal line profile of the scintillator elements under ¹³⁷Cs excitation;

Bottom: Energy spectra of 2 pixels.

Conclusions

Pixel size of GAGG:Ce array	R%@ 511keV	PV ratio	Sp. R in mm	R %@ 662keV	PV ratio	Sp. R in mm
1x1x10 mm ³	16.9	1.75	0.81	14	1.85	0.77

✓The acquired raw images of the GAGG:Ce crystal array show a visualization of all (12x12=144) discrete scintillator elements under ²²Na and ¹³⁷Cs irradiation.

- ✓ The mean energy resolution was measured equal to 16.9 and 14 for ²²Na and ¹³⁷Cs respectively.
- ✓ The mean peak to valley ratio of the profiles on the image was measured equal to 1.75 and 1.85 for ²²Na and ¹³⁷Cs.
- ✓The intrinsic spatial resolution was calculated in vertical and horizontal lines equal to 0.81mm and 0.77mm for ²²Na and ¹³⁷Cs respectively.

Acknowledgement

«This research is implemented through IKY scholarships programme and co-financed by the European Union (European Social Fund - ESF) and Greek national funds through the action entitled "Reinforcement of Postdoctoral Researchers", in the framework of the Operational Programme "Human Resources Development Program, Education and Lifelong Learning" of the National Strategic Reference Framework (NSRF) 2014 – 2020».

References

- 1. Buzhan, P., L. Filatov, A. Ilyin, V. Kantzerov, V. Kaplin, A. Karakash, F. Kayumov, S. Klemin, E. Popova, and S. Smirnov, (20B. Dolgoshein, 03) "Silicon photomultiplier and its possible applications." *Nucl. Instrum. Methods Phys. Res. A*, Vol. 504, pp.48-52.
- Fysikopoulos E, Loudos G, Georgiou M, David S, Matsopoulos GA. Spartan 6 FPGA-based data acquisition system for dedicated imagers in nuclear medicine. Meas Sci Technol 2012; 23(12). <u>http://dx.doi.org/10.1088/0957-0233/23/12/125403</u>.
- 3. M. Streun ,G. Brandenburg , H. Larue, E. Zimmermann, K. Ziemons and H. Halling, (2001) "Pulse Recording by Free-Running Sampling", *IEEE Trans. Nucl. Sci.*, vol. 48, pp. 524-526,
- V. Popov, S. Majewski and B. Welch, (2006) "A novel readout concept for multianode photomultiplier tubes with pad matrix anode layout", *Nucl. Instrum. Meth. A*, Vol. 567, p. 319
- Yamamoto, S., Imaizumi, M., Watabe, T., Watabe, H., Kanai, Y., Shimosegawa, E., Hatazawa, J., 2010. Development of a Si-PM-based high-resolution PET system for small animals. Phys. Med. Biol. 55, pp. 5817-5831

